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Calculation of Resistive Loads for Elastic Resistive Exercises

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1 ABSTRACT

2 **Context:** What is the correct resistive load to start resistive training with elastic resistance to 3 gain strength? This question is typically answered by the clinician's best estimate and patient's level of discomfort without objective evidence. **Objective:** To determine the average level of 4 5 resistance to initiate a strengthening routine with elastic resistance following isometric strength 6 testing. **Design:** Cohort. **Setting:** Clinical. **Participants:** Thirty-four subjects (31±13yrs, 7 73 ± 17 kg, 170 ± 12 cm). **Interventions:** The force produced was measured in Newtons (N) with an 8 isometric dynamometer. The force distance was the distance from center of joint to location of 9 force applied was measured in meters to calculate torque that was called "Test Torque" for the purposes of this report. This torque data was converted to "Exercise Load" in pounds based on 10 the location where the resistance was applied, specifically the distance away from the center of 11 rotation of the exercising limb. The average amount of exercise load as percentage of initial Test 12 Torque for each individual for each exercise was recorded to determine what the average level of 13 14 resistance that could be used for elastic resistance strengthening program. Main Outcome Measures: The percentage of initial test torque calculated for the exercise was recorded for each 15 16 exercise and torque produced was normalized to body weight. **Results:** The average percentage of maximal isometric force that was used to initiate exercises was $30 \pm 7\%$ of test torque. 17 **Conclusions:** This provides clinicians with an objective target load to start elastic resistance 18 19 training. Individual variations will occur but utilization of a load cell during elastic resistance provides objective documentation of exercise progression. 20

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24 INTRODUCTION

25 Elastic resistance training is commonly used to increase muscular strength in orthopedic and sports rehabilitation. Muscular strength gains are effectively increased through various 26 modes such as free weights or elastic resistive bands. ¹⁻³ A critical challenge for clinicians is to 27 28 determine what resistive load should be used to begin an effective strengthening intervention, 29 particularly when using elastic resistive modes of exercise. The isotonic literature suggests using 30 a one-repetition maximum (1RM) to determine the appropriate load to use for strength training,^{4,5} then applying a load between 50-80% of 1RM to facilitate strength gains.^{6,7} 31 Unfortunately, this approach is more suited for large muscle groups during bench press or squats 32 which are not as applicable for rehabilitation based strengthening interventions for individuals 33 just starting resisitive exercises or for single-joint motions. Strength testing in the rehabilitation 34 setting is more commonly performed using isometric dynamometers and method to convert 35 isometric strength measures to exercise resistive loads is not well established. 36

37 Currently there is a gap in the rehabilitation literature as to what specific resistive loads should clinicians prescribe for single-joint exercises used in rehabilitation. Typically patients are 38 39 given specific exercises such as shoulder external rotation, not bench press, to strengthen injured 40 shoulders. Clinicians often use isometric dynamometers instead of isotonic 1RM to evaluate strength capacity. It is unknown if 50% or another percentage should be used for prescribing 41 42 resistance loads for isotonic elastic resistance exercises without compensation. Testing isometric strength makes it difficult to find a load that is then appropriate for isotonic exercise. The 43 44 literature is limited in how to convert an isometric strength measurement to estimate the resistive load to begin exercises, especially with resistance bands. In order to address these and provide 45 clinicians with a means to accurately prescribe effective isotonic elastic exercise loads following 46

an isometric strength assessment we propose the following study with two aims: 1) to determine
the average initial resistive loads used by participants performing isolated exercise motion using
elastic resistance and 2) to provide a calculation and matrix for clinicians to assist in determining
what loads to start their patients.

51 METHODS

52 Design and Participants

This is a cohort study undergoing a secondary analysis from another clinical trial (In 53 54 process, Journal of Strength and Conditioning Research). The larger clinical trial examined the 55 effectiveness of using a load cell with elastic resistance in strength gain and rate of strength gain compared to no load cell. Thirty-four healthy volunteers, 10 males and 24 females, (31±13 years, 56 170±12cm, 72.9±17.4 kg) signed a university approved consent form to participate in an eight 57 58 week study to gain strength in their shoulders and hips. Our participants ranged in training levels 59 from sedentary to moderately active at baseline based on measures from the Marx Shoulder Activity Scale⁸ and Marx Activity Scale,⁹ averaging 9 ± 4 and 5 ± 5 points respectively. The Marx 60 Shoulder Activity Scale ranges from 0-20 points, a higher score indicating a more active 61 individual. The Marx Activity Scale, a lower extremity activity scale, ranges from 0-16. The 62 higher the score on the Marx Activity Scale the higher the activity level. 63

64 Procedures

Study participants underwent baseline isometric strength assessment prior to starting the
eight week elastic resistance training program. The details of the training program are presented
in the clinical trial. All elastic resistance exercises were completed using a load cell (Roylan
Smart Handle®, Patterson Medical Supply, Chicago, IL, USA) to allow for a set load for each

exercise. The load cell provided the participant and clinician with exact resistance load being
used. The load cell provided an auditory feedback in the form of a beep when the targeted load
was obtained. The auditory feedback was maintained as long as the targeted load was meet or
exceeded providing some level of motivation for the patient achieve the auditory target.

73 Isometric Strength Testing

All strength testing was performed on the BTE Primus (BTE Technologies, Hanover, 74 MD). Baseline strength testing for bilateral shoulder external rotation, shoulder abduction, hip 75 abduction and hip extension was measured in Newtons (N) and the lever arm distance where 76 force was applied from the center of joint rotation for the limb was measured in meters to 77 determine torque produced in Newton-meters (Nm). Each participant was allowed to familiarize 78 79 themselves with the strength testing positions prior to performing two maximal efforts for five seconds with thirty second rest between trials for all positions (Table 1).^{10,11} Participants were 80 instructed to gradually increase their force produced to reach maximum contraction during 81 82 familiarization and testing. The average of the two trials was used to represent a participants' level of strength for each position. Procedures were repeated at subsequent two week intervals 83 using the same instructions and positions for the 8 weeks of training. Prior to starting the study 84 the inter-day reliability was established for testing procedures. The intraclass correlation 85 coefficients (ICC) for average percent of body weight generated were found to be highly reliable 86 (0.91-0.95) for all tests. 87

Prior to strength testing, each subject was measured with a standard cloth tape measure to determine the lever arm lengths to determine resistive exercise loads. Shoulder external rotation lever arm was the distance from third metacarpal to the lateral epicondyle. Shoulder abduction was the distance from the third metacarpophalangeal joint to acromion. Hip abduction and
extension was the distance from the lateral malleolus to the top of the greater trochanter. This
was a crucial part of this study to accomplish our goals. We have determined that using subject's
height makes this step unnecessary and will be detailed in the discussion.

95 Calculation of Resistive Loads for Elastic Resistive Exercises

The primary aim of this technical report is to describe this calculation process. Multiple 96 items had to be considered to calculate the "Exercise Load" to present as options to the 97 participant when starting their exercise routine. The primary challenge and key clinical point is 98 that lever arm during the exercise may not be same as lever arm during testing. Using previous 99 established testing procedures from the literature^{10,11} 3 of 4 testing positions to collect force data 100 101 was different from where the exercise load would be applied during the exercises. Although not always appreciated during strength testing with a dynamometer the force generated during 102 testing is dependent on lever arm length. Therefore, the torque generated during testing "Testing 103 104 Torque" had to be converted into an understandable value for patients that we called "Exercise Load." The exercise loads could then be presented to the patients as percentages of maximal load 105 106 produced to determine the average initial resistive load used during elastic resistance training, this study's primary aim. 107

108 The Test Torque in Newton-meters (Nm) was determined by multiplying the participants 109 force (N) by the lever arm distance (m) for each of the test positions. For demonstration purposes 110 we have selected one of our 5' 2" participants. Their values from a hip abduction test will be 111 provided for this example. Hip abduction was tested side lying (Figure 1) and dynamometer

112	placed just above the knee, lever arm = $0.33m$. The participant averaged 517 N for their testing
113	torque from their two trials:
114	Equation one: Force (517 N) x BTE Lever Arm (.33m) = Test Torque (170.6Nm)
115	To determine the "Exercise Load", first, the "Test Torque" in Nm was converted to
116	"Exercise Load" in pounds. Then we calculated multiple percentages (50%, 33%, 25%, and
117	15%) to determine which load was appropriate for an individual to start resistive exercises
118	(Figure 2). The Exercise Lever Arm for hip abduction was the distance from the greater
119	trochanter to the lateral malleolus = .73m. Converted Newtons to pounds a constant value of
120	4.45N was used in this conversion.
121	Equation two: Test Torque (170.6Nm)/Exercise Lever Arm (.73m) = (233.7N)/4.45N= "Exercise
122	Load" (52.5lbs)
123	The Exercise Load was divided into 4 percentages (50%, 33%, 25%, 15%) to provide a
124	range of values for patient.
125	Equation three: Exercise Load 52.5 lbs*percentage (.33) = "Resistive load" (17.3lbs)
126	Participants were presented loads in descending order. Participants performed exercises
127	under supervision of certified athletic trainer and asked which load they could use to perform 3
128	sets of 10 repetitions with proper form at a moderate to difficult intensity. Three sets of 10 was
129	the volume chosen for consistency in the larger study, as we did not want volume to change
130	between subjects. The initial resistance load was recorded at baseline into an excel database.
131	RESULTS

To determine the average starting loads for each isotonic exercise, descriptive analysis using means, standard deviations and 95% confidence intervals were calculated from the 30 participants. The average initial resistive loads used by participants for all exercises clustered around $30 \pm 7\%$ of the maximal exercise load (Table 2). Over subsequent weeks participants worked at an increasesed percent of their baseline measure (Table 3).

137 DISCUSSION

This is one of the first studies to use a load cell to record the initial load used during 138 elastic resistance exercise. This study provides the clinician with the knowledge that a starting 139 goal of approximately 30% of maximal isometric force generated is a reasonable and appropriate 140 load to begin a progressive resistive exercise training program. The starting loads examined were 141 142 consistently 30% of maximal isometric force for all four exercises (Table 2). This adds new 143 information that can be used in the rehabilitation setting when isometric force measures are used instead of 1RM for isotonic exercises. The use of 30% of maximal isometric force initially 144 145 appears to be adequate as strength gains were observed for both upper and lower extremity muscle groups over the course of the training program. There were average strength gains 146 ranging from 14-26% among the 30 participants (Table 3). 147

Current literature does not provide a means of converting an isometric strength test to an isotonic exercise. The clinician is faced with the dilemma as to how much resistance should be given for a prescribed training program. With the assistance from the load cell attached to the elastic resistance, we were able to determine that 30% of testing force appeared to be a reasonable and appropriate starting point for shoulder and hip resistive exercises. This study necessitated a means to convert an isometric torque measure to an isotonic resistive load, reiterating the importance of the lever arm. Although clinicians have access to manufactures
reference loads for elastic resistance, it is typically not referred to and adding a load cell
simplifies the process and provides accurate objective loads.

The isometric contraction likely accounts for the percentage used to start training. It was quickly apparent that participants could not correctly perform isotonic exercises at 50% of an isometric maximal force as it was too difficult. As mentioned previously a 1 RM is rarely appropriate in the rehabilitation setting. Isometric contractions allow for greater force being produced compared to an isotonic contraction associated with a 1 RM tests due to the forcevelocity relationship .¹² This would explain why the starting loads were 30% of an isometric maximal force.

164 This paper provides the steps necessary to convert Test Torque to Exercise Load which was done for this project. However, all the steps and procedures are not practical in a clinical 165 setting. Based on our observations of this study and relatively consistent starting loads around 166 167 30%, we created a clinician friendly matrix for shoulder and hip muscle strengthening exercises. (Table 4 and 5). The matrix takes into consideration the following factors, subject height, 168 169 location of strength testing application, and force produced during strength testing. In this study 170 we measured specific limb lengths; however, when we compared our measurements to published anthropometric measures,¹³ we observed nearly perfectly match which allows for a simplified 171 approach to be developed. We found that knowledge of patient height, force produced, and 172 location of applied resistance (above elbow or knee, above wrist or ankle) then clinician can use 173 the matrix to start resistive exercise program. There is no need for the clinician to measure the 174 exercise lever arm individually. We chose the 5th, 50th, and 95th percentile of the male national 175 average as heights as there was only minimal differences between men and women.¹⁴ As 176

demonstrated by the tables there are slight differences between heights, so for simplicity we 177 provided only 3 heights representing 90% of the population. Using our previously mentioned 178 participant above, at 5' 2" with a strength measurement of 517N (116 lbs) of hip abduction, a 179 180 clinician could use Table 5 to begin the participant at approximately 15.5 lbs for exercise with load at the ankle. Although this does not address all exercises it is reasonable that 30% of 181 maximal force produced would apply to many individuals starting a resistance training program. 182 Obviously individual variations will occur based on specific patient situations and pain levels. 183 This study address the primary objective to provide clinicians with an average initial resistance 184 loads for both elastic and weight training exercises following isometric strength testing. 185

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